

ADVANCED RECONSTRUCTION TECHNIQUES IN MRI - 2

Presented by
Rahil Kothari

PARTIAL FOURIER RECONSTRUCTION

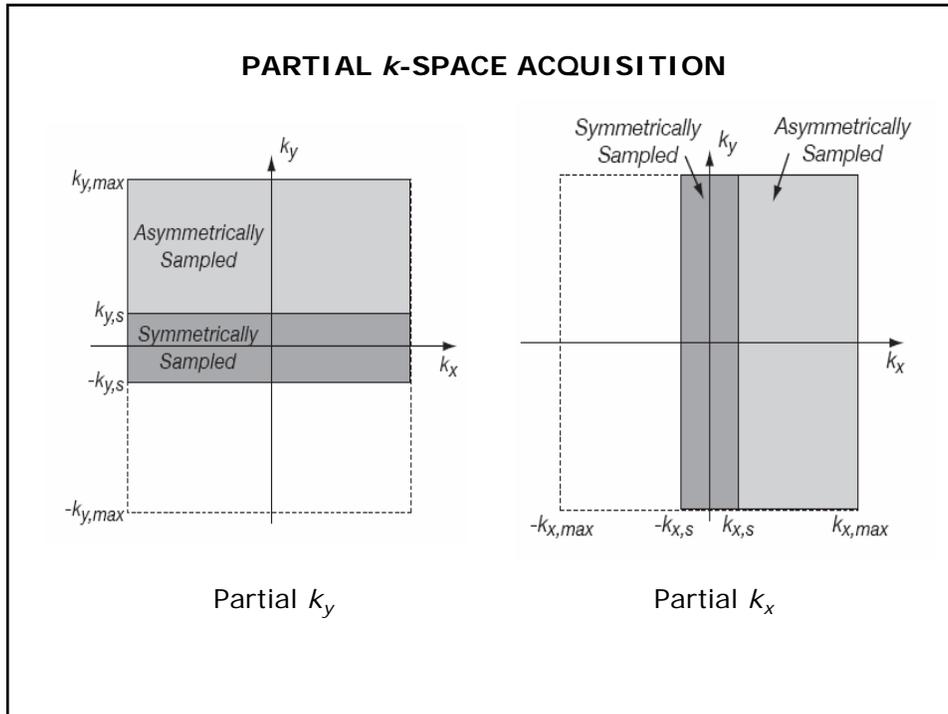
WHAT IS PARTIAL FOURIER RECONSTRUCTION?

- In Partial Fourier Reconstruction data is not collected symmetrically around the center of k -space.
- This method takes advantage of the fact that, if the image is real, the Fourier Transform is Hermitian

$$S(-k_x, -k_y) = S^*(k_x, k_y) \quad \dots(1)$$

** denotes the complex conjugate*

- Thus, one half of the k -space is completely filled, and a small amount of additional data from the other half is collected.



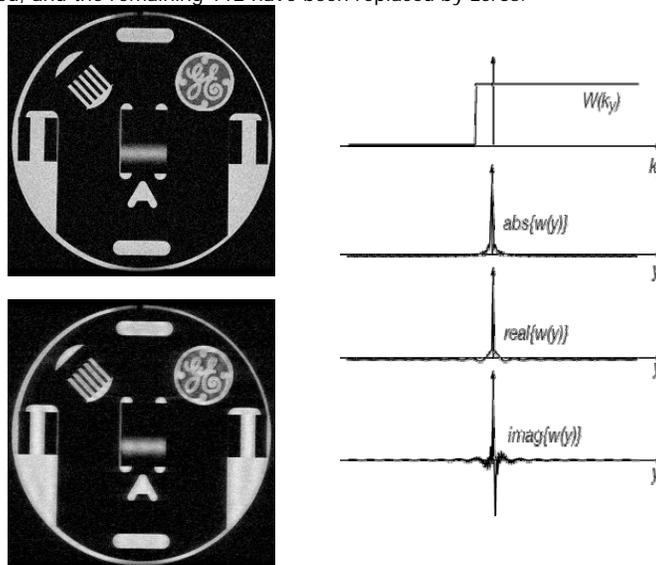
SO WHY SAMPLE MORE THAN HALF THE k -SPACE?

- MRI is an image of weighted spin densities $\rho(x)$ as a function of position.
- But there are unwanted phase shifts resulting from motion, resonance frequency offsets, hardware delays, eddy currents, and B1 field inhomogeneity.
- These cause the signal to be complex instead of being purely real.
- The data collected in the incompletely filled half of k -space shown is used to overcome the problem.

ZERO FILLING

- The simplest way to reconstruct a partial k-space data set is to simply fill the uncollected data with zeroes.
- After filling with zeroes, we perform the standard 2D Fourier Transform and display the magnitude.
- This results in Gibbs ringing near the sharp edges due to truncation of k-space data.
- This works acceptably if the collected k-space fraction is close to 1, and works poorly as this fraction approaches 0.5. Usually, a reasonable phase accuracy is achieved by acquiring a relatively high fraction of k-space, greater than 0.75.

Fig. 1 Comparison of a reconstruction of a full k-space data, and a trivial partial k-space reconstruction of the same data set where only 144 of 256 phase encodes have been used, and the remaining 112 have been replaced by zeros.



HOMODYNE PROCESSING*

- Homodyne processing uses low spatial frequency phase map generated from the data itself to correct for phase errors produced by the reconstruction of incomplete k-space data.
- Homodyne processing exploits the Hermitian conjugate symmetry of k-space data that would result if the reconstructed object were real.

* Noll et al., 1991

Mathematical Explanation

Consider a 1-D case. Let the k-space data $S(k)$ for full Fourier acquisition extend from $-k_{max}$ to $+k_{max}$. Suppose, in the partial Fourier acquisition, k-space data is acquired from $-k_0$ to $+k_{max}$ where k_0 is positive. It can be assumed that k-space data is sampled symmetrically about the low frequency region between $(-k_0, +k_0)$ around $k=0$ and sampled unsymmetrically about the high frequency region between (k_0, k_{max}) .

Now, the algorithm is divided into 2 steps:

1. Hermitian Conjugate Replacement of missing data
2. Correction for the Imaginary Component

Hermitian Conjugate Replacement:

Assuming an ideal case – for symmetrically sampled k-space data, the reconstructed image is real and is given by,

$$I(x) = \int_{-k_{max}}^{+k_{max}} S(k) e^{j2\pi kx} dk \quad \dots(2)$$

Data in the range $(-k_{max}, -k_0)$ can be replaced by complex conjugate of data in the range (k_0, k_{max}) , resulting in,

$$I(x) = \int_{-k_{max}}^{-k_0} S^*(-k) e^{j2\pi kx} dk + \int_{-k_0}^{+k_{max}} S(k) e^{j2\pi kx} dk \quad \dots(3)$$

In the first term, let $k' = -k$, resulting in,

$$I(x) = \int_{-k_{max}}^{-k_0} S^*(k') e^{-j2\pi k'x} (-dk') + \int_{-k_0}^{+k_{max}} S(k) e^{j2\pi kx} dk \quad \dots(4)$$

Thus,

$$I(x) = \left[\int_{k_0}^{k_{max}} S(k') e^{j2\pi k'x} dk' \right]^* + \int_{-k_0}^{+k_{max}} S(k) e^{j2\pi kx} dk \quad \dots(5)$$

The second term can be split into two, between $(-k_0, k_0)$ and (k_0, k_{max}) . Combining the second of the two terms with the first term, gives,

$$I(x) = \int_{-k_0}^{+k_0} S(k) e^{j2\pi kx} dk + 2 \operatorname{Re} \left[\int_{k_0}^{k_{max}} S(k) e^{j2\pi kx} dk \right] \quad \dots(6)$$

Since, the sum of a complex number and its conjugate is equal to twice the real part. Thus, the second term is real by definition, and since we assume that final image $I(x)$ is real, first term must also be real. Therefore,

$$I(x) = \text{Re} \left[\int_{-k_0}^{+k_0} S(k) e^{j2\pi kx} dk + 2 \int_{k_0}^{k_{max}} S(k) e^{j2\pi kx} dk \right] \dots(7)$$

Which can be further simplified by defining a function $H(k)$ given as,

$$H(k) = \begin{cases} 0 & k < -k_0 \\ 1 & -k_0 \leq k < k_0 \\ 2 & k \geq k_0 \end{cases} \dots(8)$$

to give, $I(x) = \text{Re}[I_H(x)] \dots(9)$

where, $I_H(x) = \int_{-k_{max}}^{+k_{max}} H(k) S(k) e^{j2\pi kx} dk \dots(10)$

The function $H(k)$ is called the Homodyne High Pass Filter.

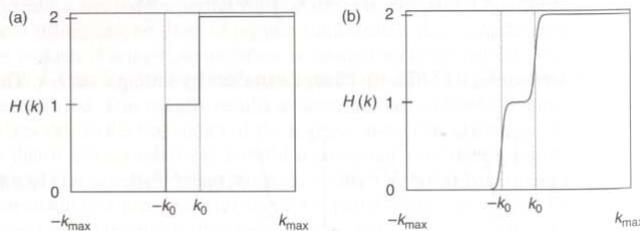


Fig. 2 Homodyne high-pass filter. (a) Conceptual version (b) Apodized version with smooth transitions.

- Eq. 9 and Eq. 10 implies that instead of using the Hermitian conjugate symmetry for reconstruction, the partial Fourier data can be reconstructed using Homodyne High-pass filter.
- This method zero fills the missing data and doubles the weighting of the asymmetrically sampled data.
- The operation of taking the real part is required because doubling the asymmetrically sampled high frequencies generates an unwanted imaginary component.
- Abrupt transitions in $H(k)$ cause ringing.

- The transition smoothing of the above filter could be obtained by using the appropriate window. The resulting Homodyne HPF would be:

$$H(k) = \begin{cases} 0 & k \leq -k_0 - w/2 \\ \cos^2\left(\frac{\pi(|k| - (k_0 - w/2))}{2w}\right) & -k_0 - w/2 < k < -k_0 + w/2 \\ 1 & -k_0 + w/2 \leq k \leq k_0 - w/2 \\ 1 + \cos^2\left(\frac{\pi(|k| - (k_0 + w/2))}{2w}\right) & k_0 - w/2 < k < k_0 + w/2 \\ 2 & k \geq k_0 + w/2 \end{cases} \dots(11)$$

Correction for the Imaginary Component:

- Since $I(x)$ is not purely real, the operation of taking the real part discards some desired signal.
- This problem can be avoided by phase correction.
- In Homodyne filtering, the phase correction is derived from the symmetrically sampled k-space data.
- A low frequency image $I_L(x)$ is reconstructed from:

$$I_L(x) = \int_{-k_0}^{+k_0} S(k) e^{j2\pi kx} dk = \int_{-k_{max}}^{k_{max}} L(k) S(k) e^{j2\pi kx} dk \dots (12)$$

where:
$$L(k) = \begin{cases} 1 & |k| \leq k_0 \\ 0 & |k| > k_0 \end{cases} \dots (13)$$

$L(k)$ is a low pass filter.

In practice, a filter with smooth transition is used.

$$L(k) = \begin{cases} 1 & |k| \leq k_0 - w/2 \\ \cos^2\left(\frac{\pi(|k| - (k_0 - w/2))}{2w}\right) & k_0 - w/2 < |k| < k_0 + w/2 \\ 0 & |k| \geq k_0 + w/2 \end{cases} \dots (14)$$

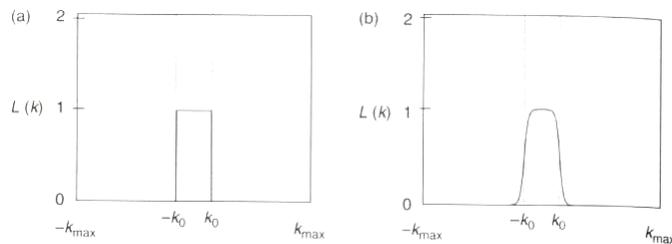


Fig. 3 Homodyne low-pass filter. (a) Conceptual version (b) Apodized version with smooth transitions.

- We approximate the phase of $I(x)$ to the phase of $I_L(x)$, denoted by $\Phi_L(x)$.
- Thus, the phase corrected image is denoted by $I_H(x)e^{-\Phi_L(x)}$ has $I(x)$ registered to the real part of the image, allowing the undesired imaginary component from the homodyne filter.
- Thus, the entire homodyne reconstruction can be expressed as

$$I(x) = \text{Re}[I_H(x)e^{-\Phi_L(x)}] \quad \dots(15)$$

- To avoid phase wrapping from using an arctangent function, it is preferable to avoid calculating $\Phi_L(x)$ explicitly. Instead, we evaluate Eq. 15 using,

$$I_H(x)e^{-\Phi_L(x)} = I_H(x) \frac{I_L^*(x)}{|I_L(x)|} \quad \dots(16)$$

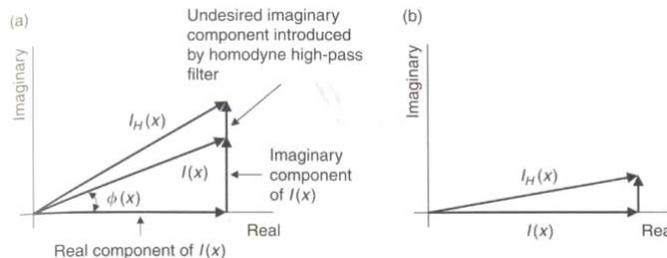


Fig. 4 Complex image value at one pixel (a) before phase correction and (b) after phase correction. $I(x)$ has phase $\Phi(x)$ which we approximate as $\Phi_L(x)$ the phase of low-pass filtered image. The phase correction removes $\Phi_L(x)$, thereby approximately registering $I(x)$ into real part of the phase corrected image $I_H(x)e^{-i\Phi_L(x)}$. This allows discarding the imaginary image component introduced by homodyne high-pass filter.

- The approximation that the phase of the image can be represented by $\Phi_L(x)$ means that homodyne reconstruction performs relatively poorly in region of rapidly varying phase caused by susceptibility changes.
- Iterative methods provide improved performance.

EXTENSION TO 2-D AND 3-D SPACE

- Earlier we considered a 1-D k-space for simplicity. Expanding to the 2-D domain

$$S(-k_x, -k_y) = S^*(k_x, k_y) \quad \dots(17)$$

- Suppose that the partial Fourier acquisition were used in both the k_x and k_y directions with partial Fourier fraction of 0.5, thus acquiring only one of the four quadrants of 2D k-space.
- Using Eq. 16 helps us fill only the diagonally opposed quadrant, leaving two other quadrants empty.
- Thus if partial Fourier is used in two orthogonal directions, one direction can be processed with homodyne reconstruction but the second direction must use zero filling.

- Conversely, if partial Fourier is used in one direction, the other k-space directions must be processed first with the normal algorithm.

- Consider a 2-D case in which full Fourier acquisition is used in k_x direction whereas partial Fourier is used in the k_y direction.

- Taking 1-D F.T. of the fully sampled k_x direction results in partially transformed data $S_p(x, k_y)$ given by,

$$S_p(x, k_y) = \int S(k_x, k_y) e^{j2\pi k_x x} dk_x \quad \dots(18)$$

where $S_p(x, k_y)$ is called the signal in hybrid space.

- The Hermitian conjugate of $S_p(x, k_y)$ with respect to k_y is,

$$S_p^*(x, -k_y) = \int S^*(k_x, -k_y) e^{-j2\pi k_x x} dk_x \quad \dots(19)$$

- Using Hermitian relationship $S^*(k_x, -k_y) = S(-k_x, k_y)$ yields,

$$S_p^*(x, -k_y) = \int S(-k_x, k_y) e^{-j2\pi k_x x} dk_x \quad \dots(20)$$

- Finally, $S_p^*(x, -k_y) = S_p(x, k_y)$... (21)

- Because the partially transformed data obeys the same Hermitian relationship as 1D k-space data, the 2D data is first processed normally in the full Fourier direction (k_x), followed by partial processing in the k_y direction.

- The extension to three dimensions is straightforward.

Fig 5. The flowchart for the same is shown below.

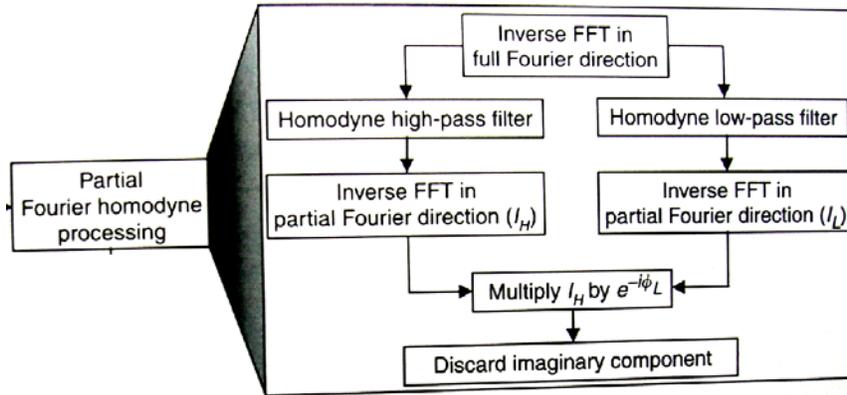
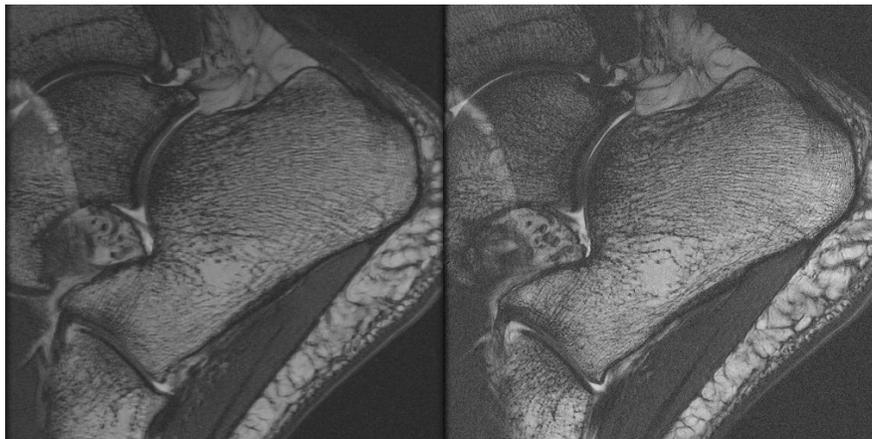


Fig. 6 Comparison between zero-filled and homodyne processing:

Zero-filled

Homodyne Processing



DISADVANTAGES OF HOMODYNE RECONSTRUCTION

- As seen in Eq. 16, image phase is lost with homodyne reconstruction. Hence it is unsuitable for applications such as shimming, phase contrast, and phase sensitive thermal imaging.

ITERATIVE HOMODYNE PROCESSING

- A drawback of the Homodyne method is that the low-frequency phase map used cannot accurately determine the rapidly varying phase.
- To address this problem, iterative partial Fourier Transform has been developed.
- In this method, an image is formed using Homodyne Reconstruction.
- This image is then Fourier transformed to obtain estimated k-space data.

- The original k-space data in the range $(-k_0, k_{max})$ are combined with the newly estimated k-space data in the range $(-k_{max}, -k_0)$ and a new complex image I' is calculated.
- A new magnitude image is formed by applying the low-frequency phase correction to I' and taking the real component, as in non-iterative homodyne reconstruction.
- This magnitude image is input to the next iteration.

Mathematical Description

- Consider 1-D case. For the first iteration, $I_0(x)$ is given by

$$I(x) = \text{Re}[I_H(x)e^{-\phi_L(x)}] \quad \dots(21)$$

- Let $S_j(k)$ be the complex k-space data estimated at step j . Iteration starts by computing $S_0(k)$. At each step:

$$S_j(k) = FT[I_j(x)e^{i\phi_L(x)}] \quad \dots(22)$$

- This function is an estimate of the k-space value for all values of k .
- However in the range $(-k_0, k_{max})$, $S(k)$ is more accurate.
- Hence we use $S(k)$ in the range $(-k_0, k_{max})$ and $S_j(k)$ in the range $(-k_{max}, -k_0)$ should yield a better-estimated image for the next iteration step.

- Combining the two data sets, creates a discontinuity at $k=-k_0$. Therefore, it is better to smoothly blend the two datasets to obtain the estimated k-space data,

$$S_{j+1} = W(k) S(k) + [1 - W(k)] S_j(k) \quad \dots(23)$$

where $W(k)$ is a merging function,

$$W(k) = \begin{cases} 0 & k \leq -k_0 - w_m/2 \\ \cos^2\left(\frac{\pi(|k| - (k_0 - w_m/2))}{2w_m}\right) & -k_0 - w_m/2 < k < -k_0 + w_m/2 \\ 1 & k \geq -k_0 + w_m/2 \end{cases} \quad \dots(24)$$

where w_m is the merging width.

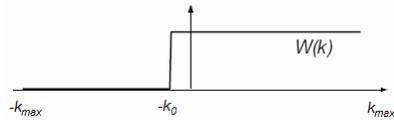


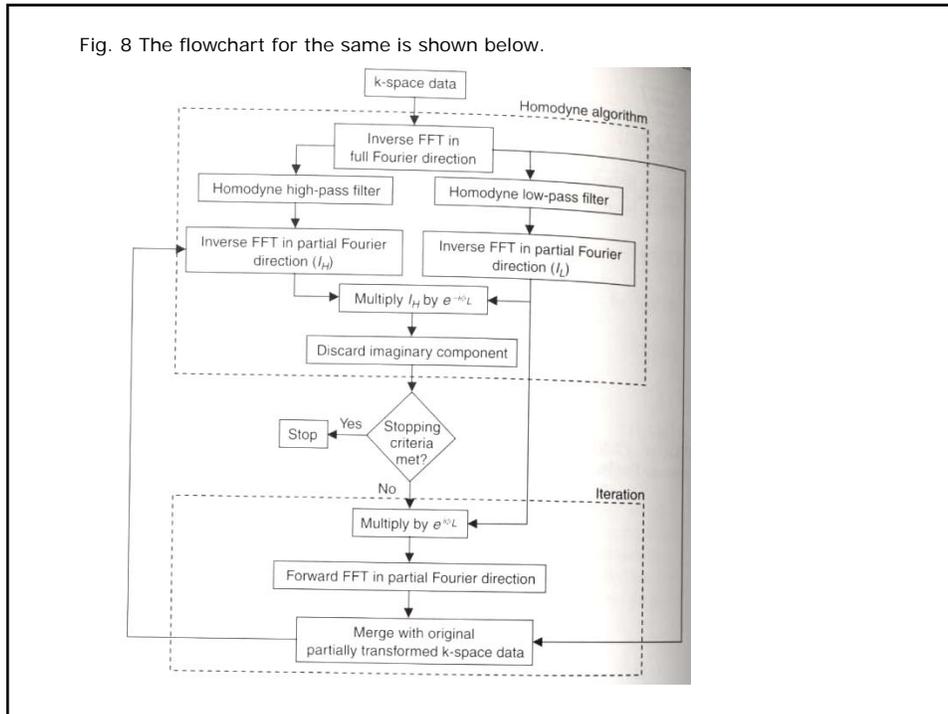
Fig. 7 Merging function $W(k)$ for iterative homodyne reconstruction

- The image for the next iteration $I_{j+1}(x)$ is:

$$I_{j+1}(x) = \text{Re}\{e^{-i\Phi_L(x)} FT^{-1}[S_{j+1}(k)]\} \quad \dots(25)$$

- Many choices for stopping criteria are possible.
 1. The algorithm continues for a fixed number of iterations.
 2. It could continue until the difference between two successive iterations becomes sufficiently small.
- Extension to 2D and 3D is similar to a non-iterative homodyne algorithm – normal reconstruction is performed first in the fully sampled Fourier directions.

Fig. 8 The flowchart for the same is shown below.



HOMEWORK #2

For the given k-space data set, perform the following:

- 1) Consider 60% of the given k-space data-set. Reconstruct the k-space using zero filing. Plot the final image thus obtained.
- 2) Consider 50% of the given k-space data-set. Reconstruct the k-space using Hermitian Conjugate Symmetry. Plot the final image thus obtained.
- 3) Consider the k-space dataset given. Generate a new k-space by taking only every 4th line from the original k-space. Plot the resultant image. What can you see?

REFERENCES

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- *Homodyne detection in Magnetic resonance imaging* in IEEE Trans. Med. Imaging 10:154-163 (1991) by Noll, D.C., Nishimura G.D., and Macovski, A.
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